

**PORTIONS
OF THIS
DOCUMENT
ARE
ILLEGIBLE**

BLANK PAGE

LA-UR-78-1769

MASTER

TITLE:

LIGHT SCATTERING WITH STREAM-IN-AIR FLOW SYSTEMS

AUTHOR(S):

J. C. Sullivan and M. L. Miller

SUBMITTED TO:

In: Proceedings of the Sixth Engineering Foundation
Conference on Automated Cytology, Elms, West Germany,
(April 20-29, 1978), Brian H. Mayall, Ed. (Journal of
Histochemistry and Cytochemistry)

In acceptance of this article for publication, the
publisher recognizes the Government's interest rights
in any copyright and the Government and its authorized
representatives have a nonexclusive right to reproduce
whole or in part said article under any copyright
secured by the publisher.

The Los Alamos Scientific Laboratory requests that the
publisher identify this article as work performed under
the auspices of the USFPA.


los alamos
scientific laboratory
of the University of California
LOS ALAMOS, NEW MEXICO 87545

Printed in the United States of America

UNITED STATES
ENERGY RESEARCH AND
DEVELOPMENT ADMINISTRATION
CONTRACT W-7405-ENG-8

Running title: Stream-in-Air Flow Systems

LIGHT SCATTERING WITH STREAM-IN-AIR FLOW SYSTEMS

G. C. Salzman and M. E. Wilder

Biophysics and Instrumentation Group, Los Alamos
Scientific Laboratory, University of California
Los Alamos, New Mexico 87545

Received for publication _____, 1978

Send proofs to: Dr. G. C. Salzman
Biophysics and Instrumentation Group (MS885)
Los Alamos Scientific Laboratory
University of California
Los Alamos, New Mexico 87545

SUMMARY

Both forward angle and 90° light-scattering measurements have been used for cell sizing with stream-in-air flow systems with very little theoretical base for the measurements. Mie theory calculations are compared with measurements on plastic microspheres. Detector response for homogeneous spheres is shown to be sensitive to refractive index, as well as to particle position within the cell stream.

Stream-in-air flow systems based on the original Stanford design (1,3) have become increasingly popular in recent years, particularly since the systems became commercially available (2,4). Both forward angle and 90° light scattering have been used with these systems for cell sizing with the assumption that the scattered light intensity increases monotonically with cell size. In this paper, we compare exact electromagnetic theory calculations for the scatter sensors used in the two commercially available cell sorters with measurements on plastic microspheres. We also present calculations showing the effects on scattered light intensity of changes in particle refractive index and particle position within the cell stream.

MATERIALS AND METHODS

In the stream-in-air flow chamber, the sample stream is surrounded by a cell-free sheath fluid and passes vertically downward through a 50- to 100- μm diameter orifice and through a focused laser beam lying in the horizontal plane a few millimeters below the orifice. Since the cylindrical stream strongly refracts and reflects the laser beam, the light collection lenses in the scatter detectors have horizontal beam stops that block the light scattered at small angles relative to the horizontal plane.

A typical forward scatter detector geometry is shown in Fig. 1 from the viewpoint of detector space. The angles θ_2 and ϕ_2 in detector space are those which would be measured if the cell stream consisted of air instead of water. H is the vertical height of the beam stop, and R_{MAX} is the effective radius of the scattered light collection lens. This radius is generally somewhat less than the full lens radius and depends on iris settings and lens mounting conditions. $D(\theta_2, \phi_2)$ is a small element on the face of the collection lens. The detector response is determined by integrating the response at D over the exposed face of the lens. Figure 2 shows the scattering geometry in cell space inside the stream. The center of the stream is at O , the laser beam is collinear with the z axis, the cell or particle is located at an arbitrary point, C , and the scattered light ray intersects the stream surface at S . The true scattering angles which are used in the electromagnetic theory scattering calculations are θ_1 and ϕ_1 . These angles depend on θ_2 and ϕ_2 but are, in general, numerically different.

For every point $D(\theta_2, \phi_2)$ in an array on the detector face, internal angles, θ_1 and ϕ_1 , are calculated using a non-linear least squares minimization code which implements the Levenberg-Marquardt algorithm (7,8). The scattered light intensity in the direction (θ_1, ϕ_1) for a homogeneous spherical particle

located at C is then calculated using exact electromagnetic theory (5,11), often referred to as Mie theory (9). The array of points, D (θ_2 , ϕ_2), consists of 20 uniformly spaced values for θ_2 and nine uniformly spaced values for ϕ_2 in the upper half plane. The calculated intensities are then averaged to give the detector response. The calculations and measurements presented are for two commercially available stream-in-air flow systems: the Becton-Dickinson FACS-II (1) and a prototype of the Coulter IPS-1 (4). In all cases, the particle volume is assumed to be uniformly illuminated at 488 nm. Imposition of a Gaussian laser beam profile will enhance the cell position effects described below.

RESULTS

Table I gives the pertinent dimensions used in the calculations. Figure 3 shows the detector response vs particle diameter as a function of particle relative refractive index for the forward scatter detectors in these two systems. The experimental data points are for plastic microspheres whose characteristics are given in Table II. The imaginary component of the refractive index was assumed to be 0.0 for all the calculations shown in the figures. The relative refractive index $m = 1.0$ corresponds to a homogeneous sphere model for a live cell, $m = 1.12$ to that for a fixed cell, and $m = 1.20$ to that for a polystyrene latex sphere immersed in a saline solution whose refractive index is 1.3345. The mismatch between theory and experiment for the 15.7- and 18- μm diameter spheres is considered in the discussion section. Note that the response is rather flat in the diameter region below 5 μm , implying that one would obtain very small light-scatter coefficients of variation for small particles with significant volume coefficients of variation. Note also that the FACS-II system is more sensitive to particle refractive index changes than is the TPS-1 system.

The forward scatter detector response is affected by the position of the particle within the stream. Figure 4 shows the calculated effects of particle position on the detector response vs particle diameter curves for the two systems for two different particle relative refractive indices. The figure legends give the coordinates of the particle center (X_C , Y_C , Z_C) in μm with respect to the center of the sample stream. These effects are illustrated more dramatically in Fig. 5 which shows a comparison between experimental and calculated scatter intensity frequency histograms for 10- μm diameter polystyrene latex microspheres (10). The calculated distributions were obtained by Monte Carlo methods using the experimental Coulter volume distributions and

the calculated position distributions. The Coulter volume frequency histogram was transformed into a diameter distribution and divided into five bins with appropriately assigned probabilities. A two-dimensional map of detector response vs particle position was generated for each diameter bin, and then an appropriate number of particles was selected at random from a normal distribution (6) with the standard deviations noted in the figure legend. The model data with 0.1- μm standard deviation reflect the particle size distribution. Only 4000 particles were used to generate this distribution to maintain a reasonable scale on the graph. The $\sigma = 0.75\text{-}\mu\text{m}$ calculations and the experimental data both contain 19,166 points.

The effects of refractive index on the 90° scatter detector response function for the FACS-II are shown in Fig. 6. The particles are assumed to be centered in the cell stream. Note that the refractive index dependence is now inverted with respect to that of the forward scatter detector. The mismatch between theory and experiment at the 15.7- and 18- μm diameters is discussed below. Figure 7 shows the effects of cell position on the 90° scatter detector response function. Particle coordinates (X_C , Y_C , Z_C) inside the cell stream are given in the figure legend.

DISCUSSION

Since the 15.7- and 18- μ m diameter spheres were darkly colored, imaginary refractive indices were chosen to minimize simultaneously the discrepancies between theory and experiment for each of these two particle sizes for the data in Figs. 3A and 3B and Fig. 6. An imaginary refractive index, n_i , of 0.0015 was successful in moving the calculation for the 18- μ m diameter spheres to within one standard deviation of the experimental data for all three detectors. An n_i value of 0.0009 moved the calculations for the 15.7- μ m diameter spheres to within 1.6 standard deviations for the FACS-II and TPS-1 forward scatter detectors. However, this correction still left the calculation for the 90° FACS-II detector seven standard deviations above the experimental data.

It has been shown that the response of scattered light detectors for two commercial stream-in-air cell sorters is sensitive both to particle refractive index and position within the stream. The effects of cell position within the sample stream can be minimized by using a concentrated sample and adjusting the sheath and sample pressures so that the sample stream diameter within the sheath stream is minimized. To address the effects of refractive index changes and non-monotonicity of the scatter detector response function, care should be taken in interpreting the data when, for example, comparing frequency histograms of cells prepared with different fixatives. Although these results are strictly applicable only to homogeneous spheres, they shed some light on problems likely to be encountered with biological cells.

ACKNOWLEDGMENTS

The authors would especially like to thank Mr. Aaron Gorman and Dr. John Kundlich of the Immunology Branch, National Cancer Institute, for providing the PMS-11 data. We would also like to thank Dr. P. P. Mahoney and M. Kozak for useful discussions, Dr. J. H. Goldstein for his interest in this work, and Mrs. Elizabeth Sullivan for preparing the manuscript, and Mr. J. H. Goldstein for photographs.

This work was performed under the auspices of the United States Department of Energy and was partially supported by the Division of Cancer Treatment and Control, National Cancer Institute, Department of Health, Education and Welfare.

Bibliography

1. Arndt-Jovin DJ, Jovin TM: Computer controlled multiparameter analysis and sorting of cells and particles. *J Histochen Cytochem* 23:627 (1974)
2. Coulter-Dickinson Electronics Laboratory, 500 Clyde Avenue, Mountain View, California 94041
3. Coulter Electronics, Inc., 11500, Laurel Way, Bala Cynwyd, Pa. 19004: Automatic cell sorting. *Rev Sci Instrum* 50:1507 (1979)
4. Coulter Electronics, Inc., 190 West 20th Street, Bialeah, Florida 33010
5. Dave JV: Subroutine for Computing the Parameters of the Electromagnetic Radiation Scattered by a Sphere. International Business Machines Scientific Center, Palo Alto, California, report 100-13 (May 1968)
6. Kieferman AJ, Kung JP: Computer generation of normal random variables. *Comm Stat A* 5: 711-801 (1976)
7. Marquardt D: An algorithm for the solution of certain non-linear problems in least squares. *J Quart Appl Math* 21:431 (1963)
8. Marquardt DJ: An algorithm for least squares estimation of nonlinear parameters. *Soc J Appl Math* 11:431 (1963)
9. Mie G: Beitrage zur Optik truerer Medien speziell kolloidaler Metalllosungen. *Ann Physik* 25:377 (1908)
10. Particle Technology, Inc., Los Alamos, New Mexico 87544 (now a subsidiary of Coulter Electronics, Inc., Bialeah, Florida 33010)
11. Stratton JA: Electromagnetic Theory. McGraw-Hill Company, New York, 1961

TABLE I

Detector Geometry Specifications Used in the Calculations

Parameter	FACS-II		
	Forward	90°	Top-3
H (mm)	1.45	0.56	2.6
R _{max} (mm)	6	3.9	10.5
Z _D (mm)	22	--	25.4
s (μm)	30	30	38.1
Y _D (mm)	--	5.2	--

TABLE 11

Physical Characteristics of the Polymers Containing Monomer 10^a

Monomer feed (mole %)		Inherent viscosity (dl/g)	
10	11	Color	Wavelength (nm)
5.0	11	Clear	19.1
7.9	11	Clear	19.3
10.0	50 _a	Pale orange	19.7
15.7	50 _a	Dark orange	20.0
18.0	70 _a	Dark red	20.2

^aThe inherent viscosities were taken at 30°C in 1,2-dichloroethane. The color was determined by measuring the absorbance at the wavelength of 486 nm.

FIG. 1. Scattering geometry as viewed from the detector space when refractive effects due to cylindrical geometry are ignored. The scattering angles θ_1 and ϕ_1 are calculated as if the cell stream were composed of air. k_{max} is the radius of the largest circle on the light collection lens such that all light passing through the circle reaches the photodetector. h is the height of the beam stop, and $D(\theta_2, \phi_2)$ is an element of area on the face of the collection lens.

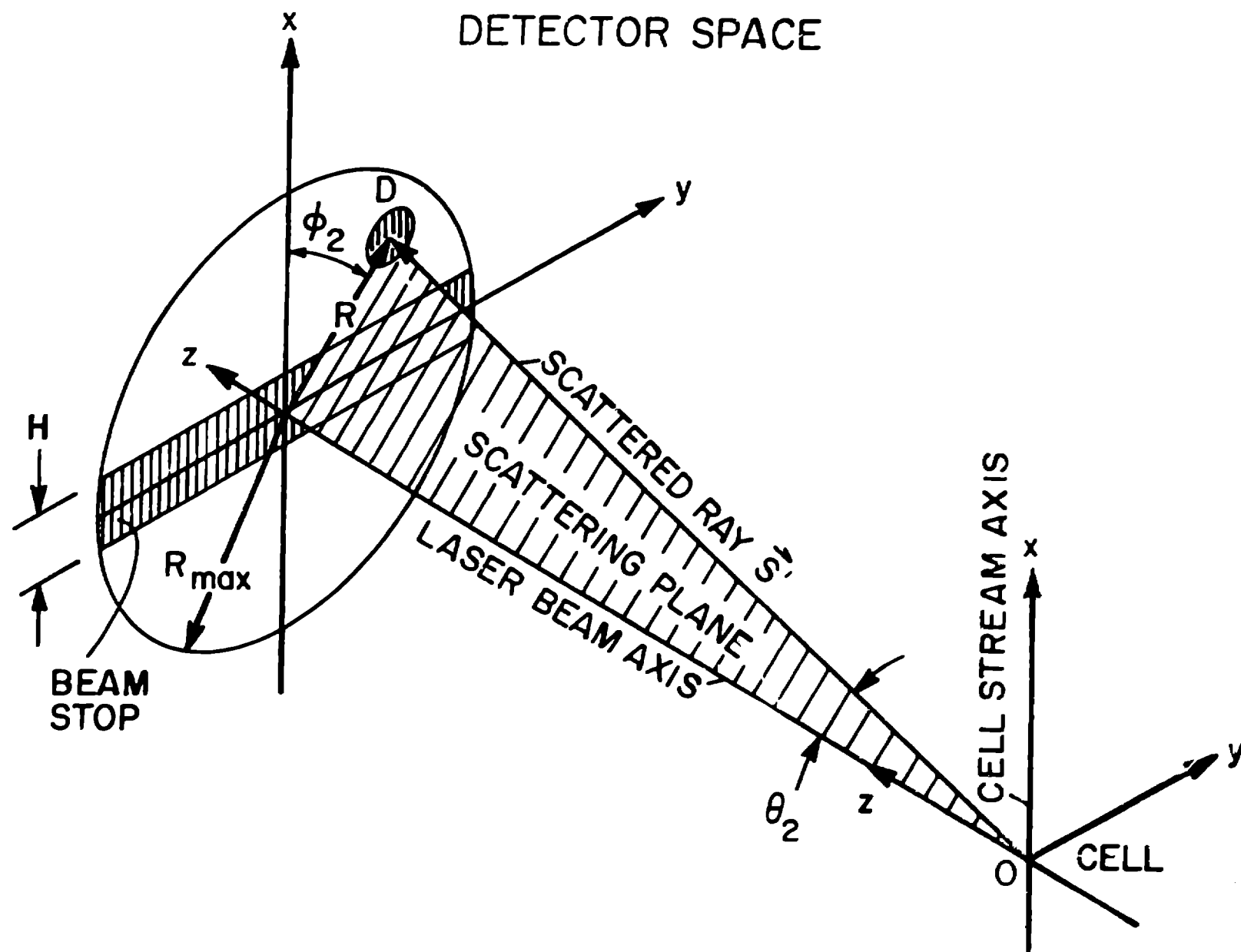


FIG. 2. Scattering geometry as viewed from the cell space inside the saline stream. The center of the stream is at O_s and the cell or particle is centered at an arbitrary point C . A scattered light ray at C is refracted at the stream boundary, S , to reach the detector at D . The internal scattering angle, θ_1 and ϕ_1 depend on θ_2 and ϕ_2 in a non-linear fashion. The stream radius is r .

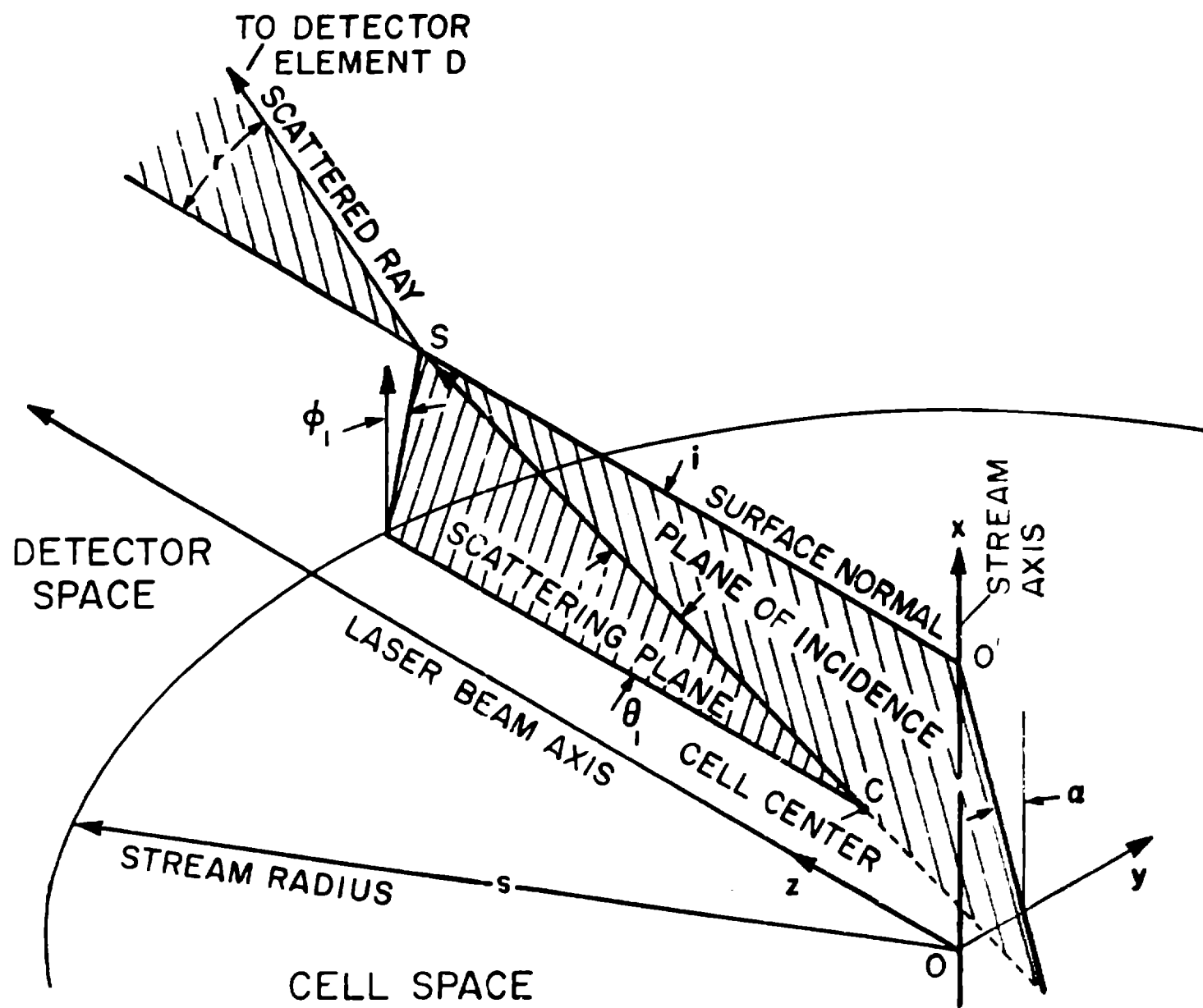


FIG. 3. Refractive index effects: Theoretical forward scatter detector response as a function of homogeneous sphere diameter for three different particle relative refractive indices, m . Experimental data points are for polystyrene latex microspheres whose properties are given in Table II. (A) FACS-II, and (B) TPS-1.

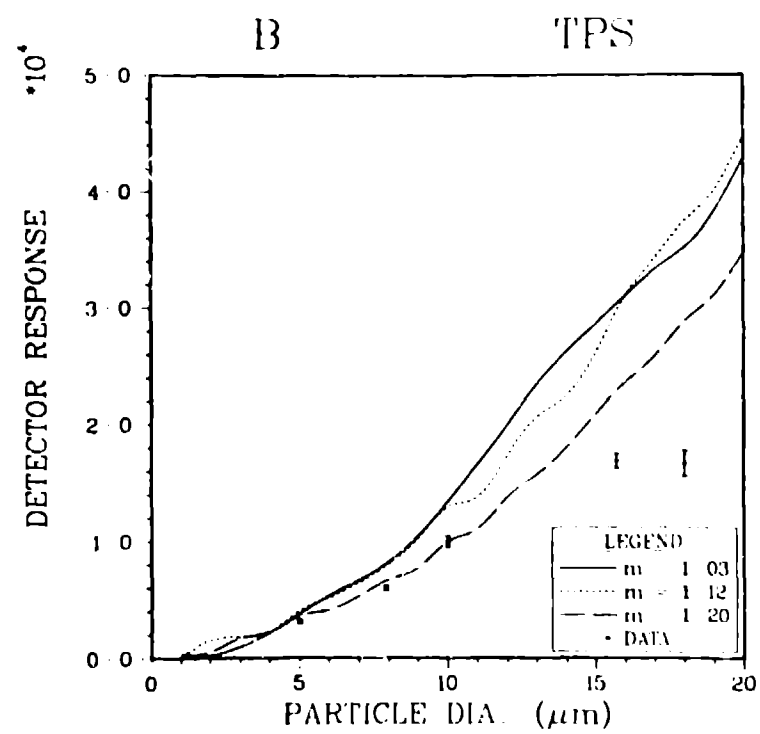
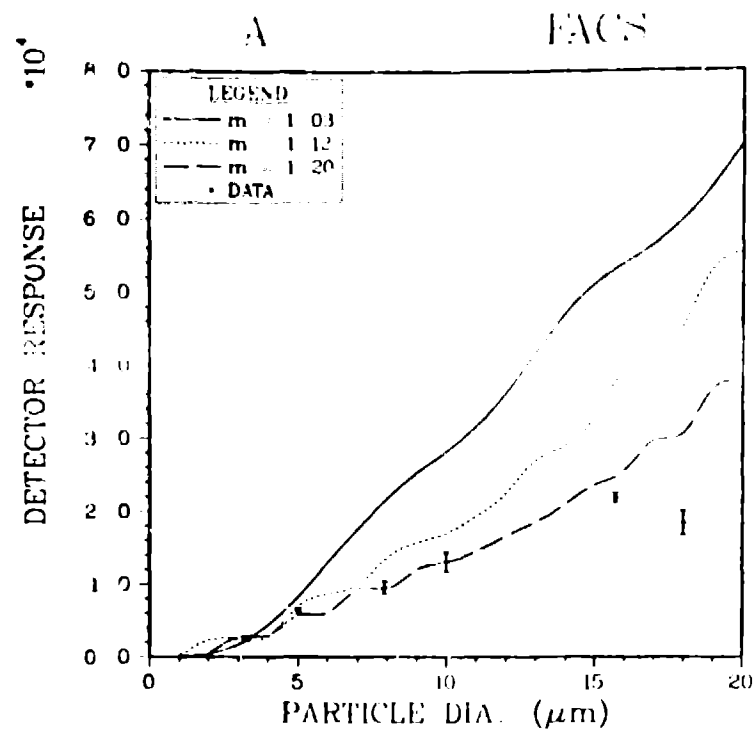


FIG. 4. Position effects: The calculated effects of particle position, C , on the forward scatter detector response vs particle diameter curves for the FACS-II and TPS-1 cell sorters for two particle relative refractive indices. The particle coordinates (X_C , Y_C , Z_C) are given in μm in the legend. (A) FACS-II, $m = 1.03$; (B) FACS-II, $m = 1.20$; (C) TPS-1, $m = 1.03$; and (D) TPS-1, $m = 1.20$.

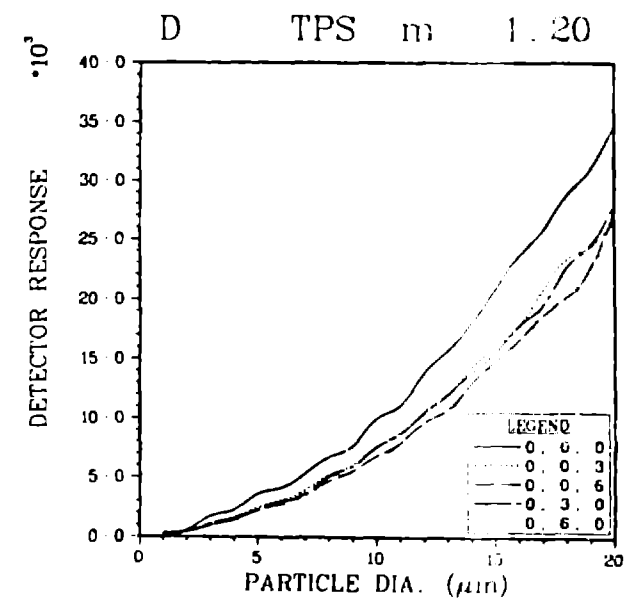
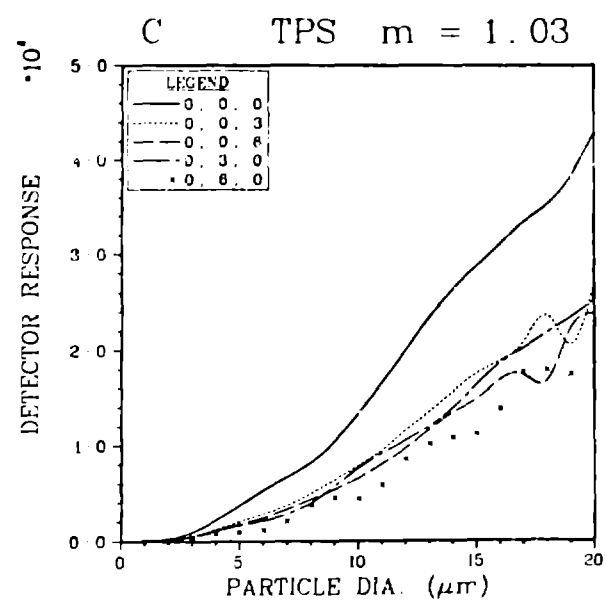
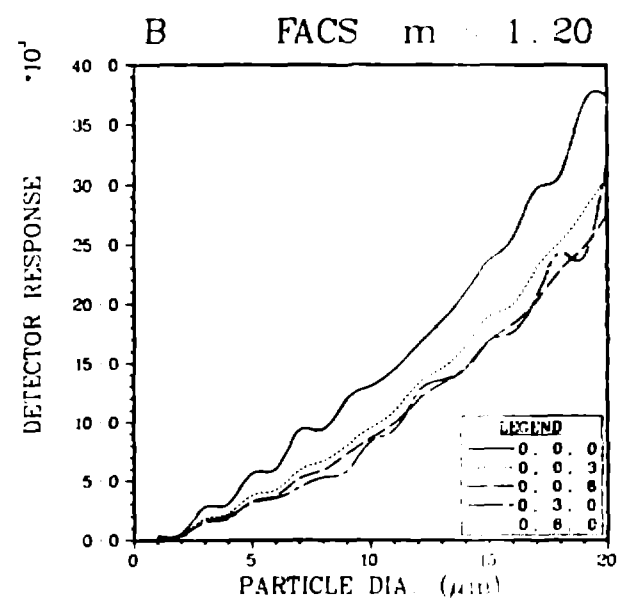
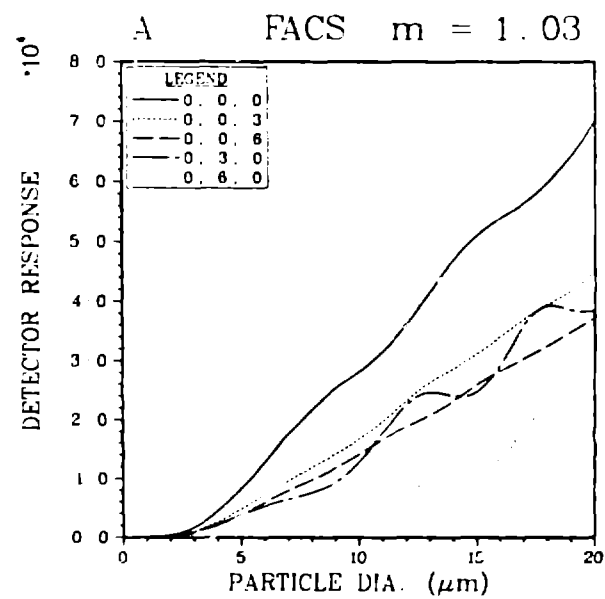


FIG. 5. Comparison between experimental and theoretical forward scatter intensity frequency histograms for 10- μ m diameter homogeneous plastic microspheres. Calculated distributions were obtained by choosing a particle at random from a normally distributed Coulter volume distribution (volume coefficient of variation 2%) and placing the particle in the Y-Z plane in the cell stream at random within a normal distribution with the standard deviations given in the legend.

FACS FORWARD SCATTER

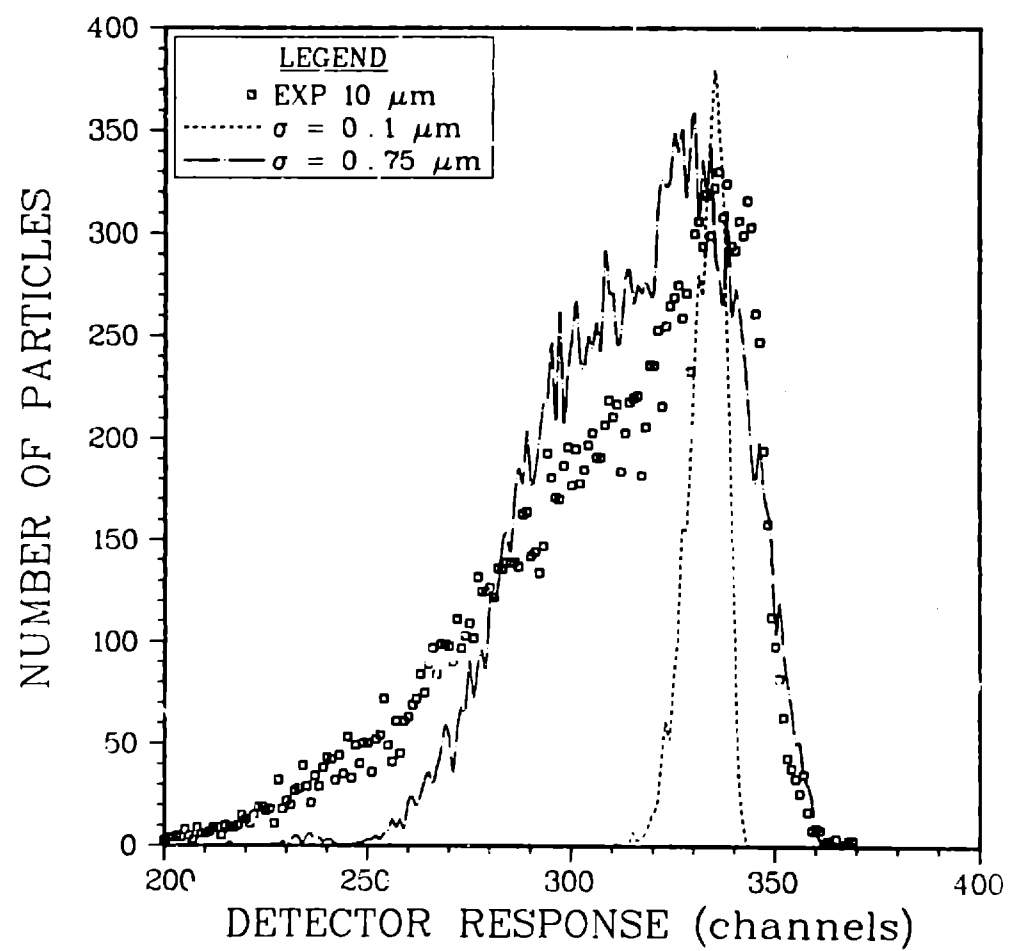


FIG. 6. Theoretical 90° FACS-II scatter detector response as a function of homogeneous sphere diameter for three particle relative refractive indices, n . Experimental data points are for uniform polystyrene latex microspheres whose properties are given in Table II.

FACS

90 DEG

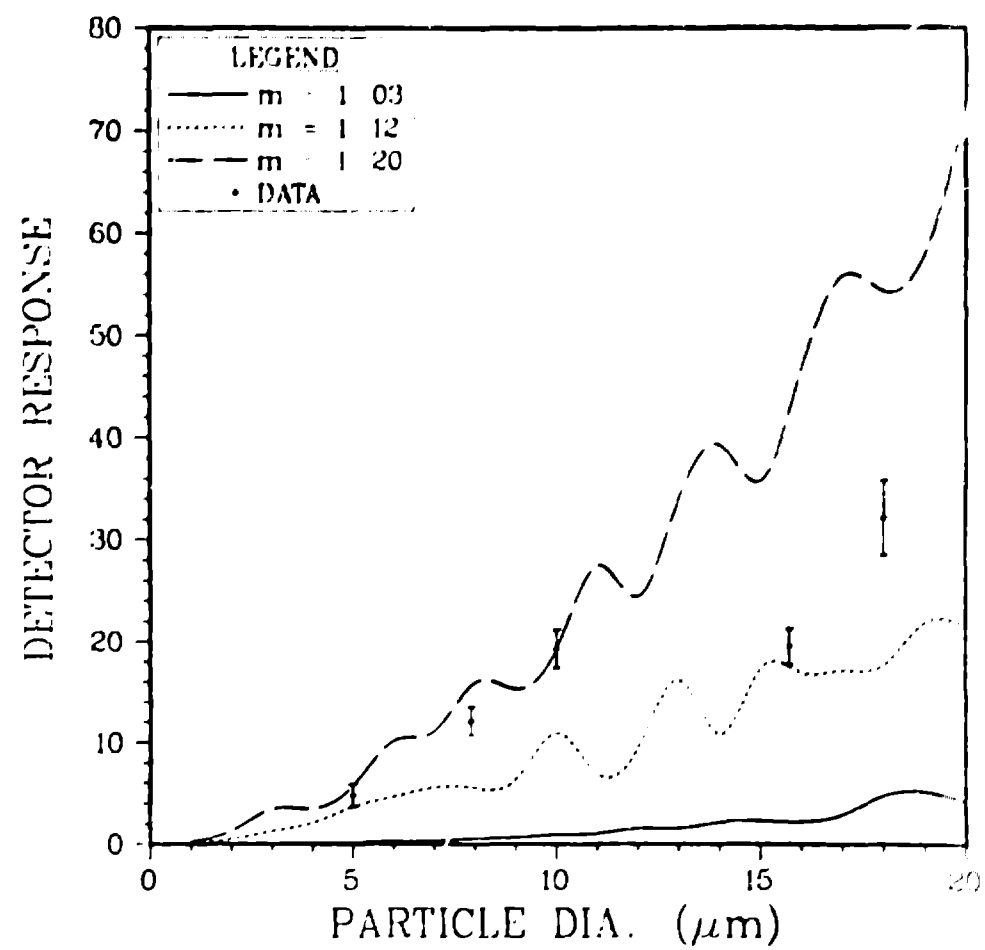
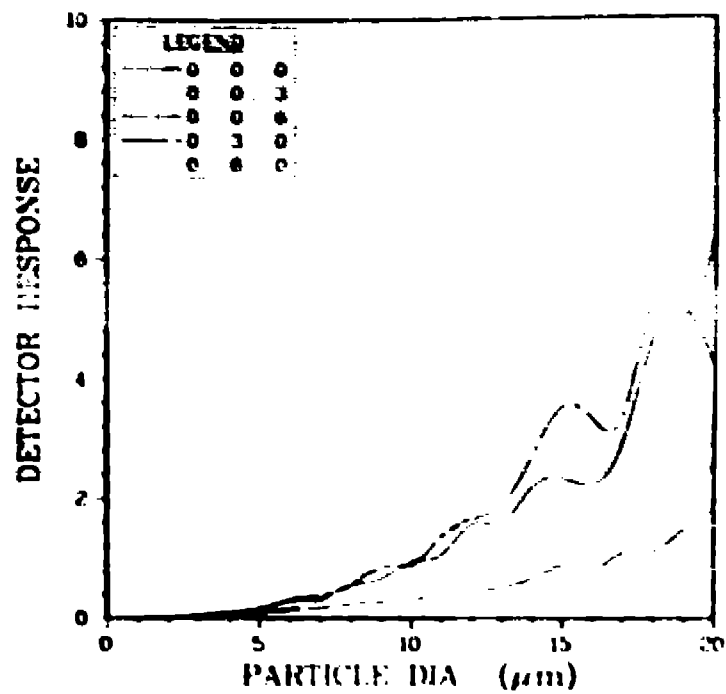


FIG. 7. The calculated effects of particle position, C , on the 90° FACS-II scatter detector response for two particle relative refractive indices, m . The particle coordinates (X_C, Y_C, Z_C) are given in μm in the legend. (A) FACS-II, $m = 1.03$; and (B) FACS-II, $m = 1.20$.

A FACS90 m 1 0.5



B FACS90 m 1 20

